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1 A Randomized Controlled Trial of PEEK vs. Titanium Interference Screws for Anterior
2 Cruciate Ligament Reconstruction with Two-year Follow-up

3
4 **ABSTRACT**

5
6 **Background:** Graft fixation with interference screws for anterior cruciate ligament
7 reconstruction is a highly successful technique. Polyether ether ketone (PEEK) is a novel
8 thermoplastic polymer with high biocompatibility, mechanical properties that mimic native
9 bone, and can be imaged on CT or MRI without signal flare.

10 **Purpose:** To compare the clinical performance of anterior cruciate ligaments (ACL)
11 reconstruction using PEEK and titanium interference screws at two years and to evaluate a
12 novel method of measuring of tunnel volume.

13 **Study design:** Randomised controlled trial; Level of evidence, 1.

14 **Methods:** 133 patients underwent arthroscopic ACL reconstruction with 4-strand hamstring
15 autografts and were randomised to have titanium or PEEK interference screws for both the
16 femoral and tibial tunnel fixation. At two years, subjective Lysholm and IKDC scores were
17 assessed, and clinical examination performed. At 12 months, MRI was performed to assess
18 graft incorporation and cyst formation, and a novel technique employed to measure tunnel
19 volumes..

20 **Results:** There were no significant difference in graft re-rupture rate, contralateral ACL
21 rupture rate, subjective outcomes or objective outcomes. In both the titanium and PEEK

22 groups, MRIs demonstrated high overall rates of graft integration (96-100% and 90-93%)
23 and ligamentization (89% and 84%), and low rates of synovitis (22% and 10%) and cyst
24 formation (0-18% and 13-15%). There is a higher proportion of patients with incomplete
25 graft integration within the femoral tunnel in the PEEK group compared with the titanium
26 group (10% vs 0%, $p=0.03$), however we suggest that metal artifact precluded proper
27 assessment by MRI of the graft in the titanium group. Tunnel volumes also appeared to be
28 equivalent in the two groups and measured using a novel technique which was highly
29 reproducible in the PEEK group secondary to the absence of flare.

30 **Conclusion:** Two-year clinical analysis of PEEK interference screws for femoral and tibial
31 fixation of ACL reconstructions showed equivalent clinical performance to titanium
32 interference screws. Given the excellent mechanical characteristics, biological compatibility
33 and absence of metal artifact on MRI, PEEK has become our material of choice for
34 interference screw fixation in ACL reconstruction.

35 **Key words:** Anterior cruciate ligament reconstruction, interference screw, Polyether ether
36 ketone (PEEK), Titanium

37 Word count: 350

38 **What is known about the subject:** Although there are several options available for fixation,
39 the use of interference screws has been shown to be highly successful and a reproducible
40 technique with excellent long-term outcomes. Polyether ether ketone (PEEK) is a
41 thermoplastic polymer which is widely used in spinal and non-orthopaedic surgery. It is
42 clinically inert, has an elastic modulus similar to bone, does not create signal flare on MRI
43 and insoluble. The use of PEEK interference screws in ACL reconstruction has not yet been

44 studied. Previous studies in cadavers and pigs have shown equivalent results in pull out
45 strength compared to Titanium interference screws.

46 **What this study adds to existing knowledge:** This study represents the first randomized
47 controlled trial to compare the clinical outcomes of PEEK and titanium interference screws.

48

49

50 **INTRODUCTION**

51

52 One of the fundamental aims of anterior cruciate ligament (ACL) reconstruction is secure
53 fixation of the graft. Although there are several options available for fixation including
54 compression, as in the use of interference screws, expansion, as in the cross-pin technic and
55 suspension with a button, there remains no definitive gold standard. This is particularly true
56 for fixation in the femoral tunnel. The use of interference screws has been shown to be
57 highly successful and a reproducible technique with excellent long-term outcomes⁴.
58 Traditionally titanium screws were used, however, due to their metallic properties, they
59 cause significant signal artifact on MRI imaging, making post-operative assessment
60 challenging⁶. Also, due to the hardness of titanium screws, damage can occur to the graft
61 during screw insertion^{22, 27}.

62

63 As the search for the ideal material has continued, “bioresorbable” interference screws
64 were theorised to solve two issues. Firstly, the material is radiologically inert and thus allows
65 for superior post-operative MRI assessment. Secondly, the bioresorbable screw would allow
66 for solid fixation, without damage to the graft as it gradually resorbs and is replaced by
67 cancellous bone. Although bioresorbable screws have been associated with good clinical
68 outcomes and do not cause MRI signal flare, resorption has proven unreliable and complete
69 replacement by bone rare⁵. This is largely due to the acidic nature of the materials and the
70 hydrolytic pathway for their dissolution resulting in bony destruction and cyst formation^{3,}
71 ²⁰.

72 Another option is polyether ether ketone (PEEK), a thermoplastic polymer which is widely
73 used in spinal and maxillofacial surgery and is becoming increasingly popular in orthopaedic
74 surgery. PEEK is chemically inert, insoluble, has a modulus of elasticity closer to human
75 cortical bone, is compatible with MRI, and, for sterilization purposes, has high resistance to
76 radiation ¹³. When compared to other commonly used materials for graft fixation, there has
77 also been shown to be no difference in tunnel widening or cyst formation^{9, 26} PEEK itself
78 does not encourage bone ingrowth or ongrowth, but it can be reinforced with elements
79 such as hydroxyapatite, carbon and tricalcium phosphate, which can encourage bony
80 incorporation. Hence PEEK represents a stable and biocompatible material that may address
81 the issues of graft damage due to material hardness, and interference with imaging, that is
82 present with titanium screws.

83

84 Previous studies in human and porcine models have shown equivalent results in pull out
85 strength between PEEK and titanium screws ^{2, 21}. Similarly, a study performed on dogs found
86 that PEEK with tricalcium phosphate fixation showed bony incorporation at six months and
87 was stable through biomechanical evaluation ¹⁶. To date the majority of the literature on
88 the use of PEEK surgical material in live humans has come from spinal and maxillary-facial
89 literature.

90

91 At present there are no prospective randomised controlled trials comparing the outcomes
92 of PEEK and titanium interference screws for ACL reconstruction. The purpose of this study
93 was to compare titanium interference screws to a novel PEEK polymer screw by randomized
94 controlled trial. The primary outcome was patient reported outcomes assessed with IKDC
95 and Lysholm score at two years. Secondary outcomes included objective measures of laxity

96 by clinical evaluation and instrumentation by KT-1000, incidence of graft rupture and MRI
97 appearance of graft integration, cyst formation and tunnel volume. We hypothesized that
98 there will be no difference in patient reported outcomes, ACL graft re-rupture rate, or
99 objective outcomes between the PEEK and titanium subjects. However, we suspected that
100 the absence of signal flare from PEEK screws will allow for more accurate MRI assessment,
101 compared to titanium screws.

102

103 **METHODS**

104

105 A parallel two group randomized controlled trial was performed on 133 patients undergoing
106 primary ACL reconstruction between September 2013 and December 2015. Patients were
107 over the age of 18, had no concomitant ligamentous injuries to the operative knee or the
108 contralateral knee, lived in the local metropolitan area and gave informed consent to
109 participate. Exclusion criteria included associated ligamentous injury to the knee, if they
110 were seeking compensation for their injury or if they were pregnant. This study was
111 performed at a high volume, private orthopaedic practice in Sydney, Australia. The surgery
112 was performed by two orthopaedic surgeons (LP, JR), using the same technique. Ethics
113 approval was sought and granted by a local ethics committee (St Vincent's Hospital, Sydney,
114 Australia).

115

116 Randomization was achieved by computer generated numbers. Prior to commencement of
117 the trial, envelopes were consecutively numbered from one to 140 with cards that
118 contained the words "TITANIUM RCI" or "PEEK RCI". Randomisation was restricted to
119 multitudes of 10 with a 1:1 allocation ratio by one researcher. On the day prior to surgery,

120 an envelope was placed into the patient's file by an administrative assistance and this was
121 opened just prior to surgery by the operating surgeon. The card was then replaced inside
122 the envelope and sealed, only to be re-opened at the conclusion of the study. Whilst the
123 surgical operator could not be blinded to the treatment group, the patient and clinical
124 assessors were.

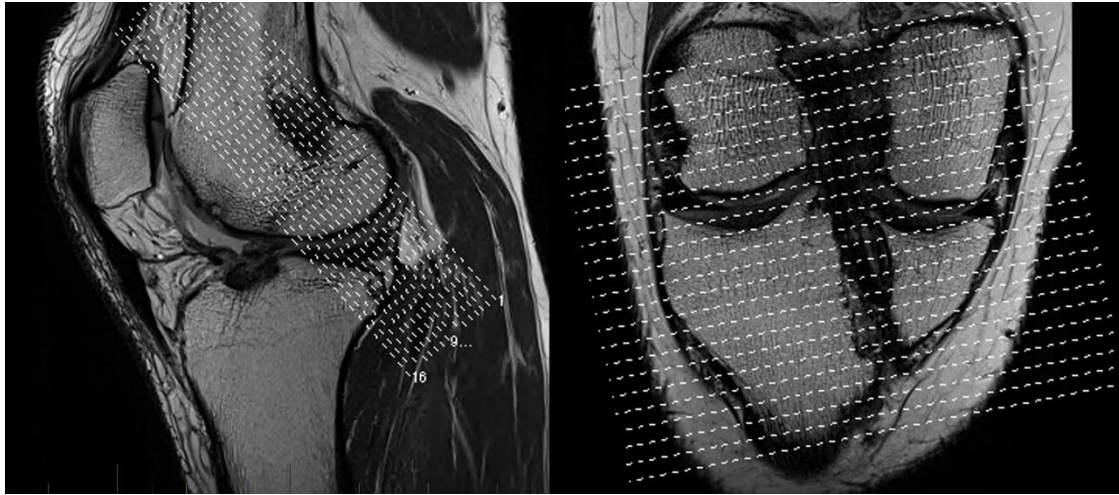
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126 All patients received 4-strand hamstring autograft with tunnels prepared by single incision
127 endoscopy technique, utilising the anteromedial portal for femoral tunnel drilling. The graft
128 was fixed at the femur and the tibia by either a PEEK RCI HA screw (Smith & Nephew,
129 Andover, Massachusetts) or Titanium RCI screw (Smith & Nephew, Andover,
130 Massachusetts). On the femoral side, a 7 X 25 mm screw was used in all patients excepting
131 one, who received an 8 X 25 mm screw. On the tibial side an 8 x 30 mm or 9 x 30 mm screw
132 was used depending on the patient's bone quality which was assessed intra-operatively by
133 manually gauging resistance when reaming. Patients in both groups were discharged home
134 on the day of surgery and underwent an accelerated rehab protocol, commencing formal
135 physiotherapy on post-operative day 0 for weight bearing and range of movement
136 exercises. Return to competitive sports was prohibited until 6-9 months after the
137 reconstruction and then was allowed only after rehabilitation goals had been met.
138 Achievement of these goals was assessed by the surgeon and the physiotherapist and
139 includes range of movement, strength and agility.

140 Standard clinical reviews took place at one week, six weeks, and six months. At 12 and 24
141 months, subjective evaluation was performed with the Lysholm questionnaire and
142 International Knee Documentation Committee (IKDC). Ligament stability was assessed with

143 a full IKDC examination, including Lachman’s test, pivot-shift test and KT-1000 arthrometer
144 (MEDmetric, San Diego, California). Assessment was performed by two specialist research
145 physiotherapists, who were blinded to screw allocation.

146 MRI was performed at one year to evaluate graft integration, the presence of effusion or
147 synovitis, cyst formation and assess tibial and femoral tunnel volumes. MRIs were
148 performed at a single imaging centre with musculoskeletal specialist MRI radiologists, and
149 modified oblique and coronal sequences chosen to optimise post-operative tunnel volume
150 measurement. If patients were unable to attend the nominated imaging centre, MRI was
151 still performed at alternate imaging centres, and all assessments were carried out by one
152 musculoskeletal radiologist except for tunnel volume measurement. Graft integration was
153 assessed on both the femoral and tibial sides by observing the graft adjacent to the
154 interference screw to have uniform, concentric low signal interface (“complete integration”)
155 or focal or diffuse high signal (“incomplete integration”) ¹⁹. The modified MRI sequences
156 were designed so that slices would be exactly perpendicular (tibial) or parallel (femoral) to
157 the long axis of the tibial and femoral tunnels; axial imaging slices were aligned
158 perpendicular to the tibial tunnel axis (“oblique axial”), and modified coronal (“oblique
159 coronal”) slices were taken parallel to the femoral tunnels (Figure 1).



160
161 Figure 1: Orientation of modified oblique sagittal (1a) and modified oblique coronal (1b)
162 MRI slices for the purposes of accurate tunnel volume assessment

163 The technique of interpretation of tunnel volume was discussed with a musculoskeletal
164 radiologist and agreed upon, then measurements were made independently by an
165 orthopaedic surgeon and an orthopaedic registrar using a computer-based volume
166 assessment tool (Intelviewer, Intelrad Systems, Montreal, Canada). For each imaging slice
167 positioned perpendicular to the femoral or tibial tunnel, the border of the tunnel was traced
168 using a stylus on a digital pen tablet device (Intuos Art, Wacom) and the cross-sectional area
169 of the enclosed region calculated. Consistent brightness and contrast ratios were
170 established (contrast/width = 1000, brightness/length = 600) such that tunnel borders were
171 clearly defined on 3mm thick proton density (PD) image slices. The tunnel cross sectional
172 area was calculated only if the full circumference of the tunnel was visible on that slice. By
173 incorporating the known slice thickness, the “Volume of Interest” tool converted adjacent
174 cross-sectional areas into a total tunnel volume (mm^3) for both the tibia and femur. The
175 technique of measurement is novel and has not previously been reported.

176

177 This study was designed to test equivalence of PEEK screws compared to titanium for the
178 primary outcome variable of mean subjective IKDC score. For a level of significance of 5%

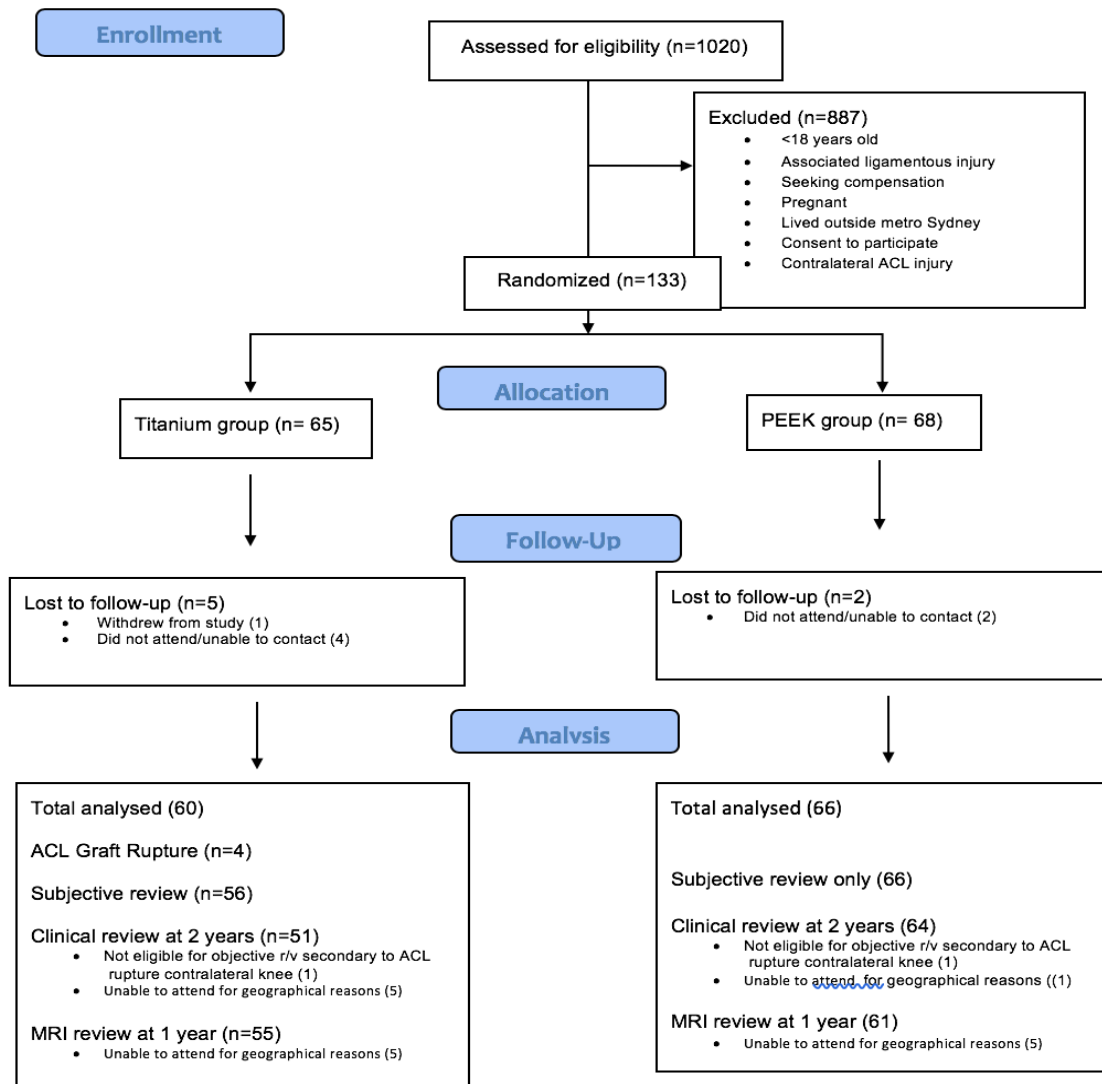
179 and power of 80%, a sample size of 53 in each group was calculated to be required to detect
180 a difference of 10%, based on a one-sided test. The sample size includes 20% oversampling
181 to allow for potential withdrawals and losses to follow-up. Statistical analysis was performed
182 with SPSS software for Windows (IBM, Armonk, NY). Statistical significance was set at P =
183 0.05. Comparison of variables between groups was analyzed with χ^2 tests for categorical
184 data and independent-samples t-test. For data elements where a count of less than 5 was
185 present in a particular category, a Fisher's Exact test was used. Linear variables were
186 summarized by the mean, and categorical variables were summarized by the frequency. To
187 assess inter-observer reliability of MRI assessment of volumes of both the femoral and tibial
188 tunnels, the intraclass correlation coefficient (ICC) was calculated. For interpretation of the
189 ICC, we used the subjective guidelines established by Landis and Koch (1977) for
190 coefficients, suggesting that values from 0.61 to 0.80 indicate "substantial" agreement
191 between observers, and values from 0.81 to 1.00 indicate "almost perfect" agreement ¹⁴.

192 **RESULTS**

193 A total of 68 patients were enrolled in the PEEK group and 65 in the titanium group. At two-
194 year review, 64 (94%) in the PEEK group and 51 (90%) in the titanium group had complete
195 subjective and objective evaluation. Two patients in the PEEK group and five in the titanium
196 group were lost to follow up and unable to be contacted. One patient in the titanium group
197 withdrew from the study, the other patients did not attend follow up or were unable to be
198 contacted. Figure 2. There was no statistical difference between groups for any of the
199 baseline patient demographics or injury profile. (Table 1).

200

201 Figure 2: Consort flow diagram



202

203

204 Table 1: Patient Demographics and injury profile

	Titanium	PEEK	p-value
Number of patients	65	68	
Mean age	33.3 (+/- 10) years	35.2 (+/- 9) years	0.26
Female	29 (44.6%)	30 (44.1%)	0.95
Left sided ACL rupture	36 (55.4%)	32 (47.0%)	0.34
Lateral meniscus injury	19 (29.2%)	17 (25%)	0.81
Medial meniscus injury	14 (21.5%)	15 (22.1%)	0.37

205

206 There was also no significant difference between titanium and PEEK groups in regards to
 207 operative tunnel volume and screw size. The mean femoral tunnel sizes at time of surgery
 208 were 7.5mm in the titanium and 7.6mm in the PEEK group (p=0.3), and the mean tibial
 209 tunnel sizes at time of surgery were 7.4mm in the titanium group and 7.5mm in the PEEK
 210 group (p=0.3).

211 There were four ACL graft ruptures over the two-year period in the titanium group, and
 212 none in the PEEK group (p=0.054). The graft ruptures occurred at three, five, nine, and 24
 213 months post-surgery, and the respective causes were fall whilst intoxicated, soccer, soccer,
 214 and fall from a ladder. Contralateral ACL rupture occurred in one patient in both the PEEK
 215 and titanium arms of the study.

216 For subjective analysis, only patients with intact ACL in the operated knee were included.
 217 This resulted in 56 patients undergoing review in the Titanium group and 66 patients in the
 218 PEEK group. There was found to be no significant difference between the two groups in
 219 regards to subjective outcomes. See Table 2.

220 Table 2: Subjective Outcomes

	Titanium Group	PEEK Group	p-value
Mean IKDC score	90 (+/- 8.9)	89 (+/- 9.1)	0.33
Mean Lysholm Knee score	94 (+/- 6.5)	94 (+/-7.2)	0.98
Return to strenuous or very strenuous activity	44 (79%)	47 (71%)	0.77
Return to pre-injury sport	42 (75%)	42 (64%)	0.16
No or mild pain with kneeling	51 (91%)	58 (88%)	0.49
No pain with strenuous or very strenuous activity	51 (91%)	48 (73%)	0.08
No swelling with strenuous or very strenuous activity	47 (84%)	53 (80%)	0.43
No giving way with strenuous or very strenuous activity	50 (89%)	57 (86%)	0.70

221

222 Objective evaluation was performed only on patients with intact graft and contralateral
 223 native ACL, this included 63 patients in the PEEK group (94%) and 53 in the titanium group
 224 (88%). Forty-two patients (79%) in the titanium group and forty-three (68%) in the PEEK
 225 group had a normal knee according to the IKDC knee examination (p=0.2). No patients were
 226 found to have an abnormal or severely abnormal knee. There was no significant difference
 227 in regards to effusion, range of movement, functional ability or degree of laxity based on
 228 Lachman’s, Pivot Shift test and KT-1000. Table 3.

229

230 Table 3: Comparison of 2 year Clinical Outcomes in the Titanium and PEEK Groups

	Titanium Group	PEEK Group	p-value
IKDC ligament grade A	42 (80%)	43 (68%)	0.18
No effusion	50 (94%)	54 (86%)	0.09
Negative Lachman test	47 (89%)	50 (80%)	0.18
Negative Pivot shift	49 (93%)	52 (83%)	0.11
KT-1000 <3mm	42 (79%)	44 (70%)	0.88
Full extension	51 (96%)	62 (98%)	0.46
Full flexion	53 (100%)	63 (100%)	1.0
Hop test >90%	40 (76%)	44 (73%)	0.32

231

232 MRIs were performed in 116 of the 133 patients (87%). Of the patients with a completed
 233 MRI, 93 (70%) had the novel modified format that allowed accurate assessment of tunnel
 234 volumes. The remaining 23 patients had MRIs performed at alternative imaging centres,
 235 with standard technique. There was no significant difference between titanium and PEEK
 236 groups in the presence of an effusion, synovitis, bone oedema adjacent to the tunnels or
 237 cyst/ganglion formation. There was a statistically significant higher rate of complete femoral
 238 graft integration in the Titanium group. Compared to the PEEK group. Table 4.

239

240 Table 4: Comparison of MRI evaluation in the Titanium and PEEK Groups

	Titanium Group (n=55)	PEEK Group (n=61)	p-value
Effusion	42 (76%)	41 (67%)	0.28
Synovitis	12 (22%)	6 (10%)	0.75
Ligamentization	49 (89%)	51 (84%)	0.39
Complete tibial integration	53 (96%)	57 (93%)	0.48
Complete femoral integration	55 (100%)	55 (90%)	0.03*
Bone oedema adjacent to tibial screw	7 (13%)	9 (15%)	0.75
Bone oedema adjacent to femoral screw	4 (7%)	7 (12%)	0.44
Cyst/ganglion tibia	10 (18%)	8 (13%)	0.45
Cyst/ganglion femur	0 (0%)	9 (15%)	0.25
Tunnel volume tibia	3.5 mm ³	3.8 mm ³	0.05
Tunnel volume femur	3.3 mm ³	2.8 mm ³	0.002*

241

242 Regarding the inter-observer reliability of tunnel volumes performed on the post-operative
 243 MRI, the intra-class coefficient (ICC) was high for the PEEK screw group; for the tibial tunnels
 244 the ICC was 0.868, and for femoral tunnels 0.689. By comparison, for the titanium screws,
 245 the ICC values were 0.768 for tibial tunnels and 0.531 for femoral tunnels. The tunnel
 246 volumes on the tibia measured an average of 3.5mm³ for the titanium group and 3.8mm³
 247 for the PEEK group (p=0.054). There was a significant difference in the volume of the
 248 femoral tunnels with the titanium group measuring an average of 3.3mm³ compared to
 249 2.8mm³ in the PEEK group (p=0.002).

250

251 **DISCUSSION**

252 The results of this study show equivalence when comparing PEEK with titanium interference
253 screws when used for ACL reconstruction, in regards to mean subjective IKDC and Lysholm
254 knee scores, re-rupture rate, and objective examination with IKDC ligament exam grades.
255 Furthermore, PEEK screws did not show any difference in rates of synovitis, oedema or cyst
256 formation on MRI compared to titanium screws at 12 months.

257 Over the 24 months there were no re-ruptures within the PEEK group. The titanium group
258 did have four patients who ruptured their graft. This result nearly approached statistical
259 significant with a p-value of 0.054. The graft ruptures from the titanium screw cohort
260 occurred at three, five, nine, and 24 months post-surgery, and the respective causes were
261 fall whilst intoxicated, soccer, soccer, and fall from a ladder. It is probable that the failures
262 were related to the nature of the mechanism of injury or ill-advised early return to sport,
263 however there is also concern that titanium screws may damage to the graft when inserted
264 and thus may contribute to early failure¹¹. A larger cohort size may have further exposed
265 this.

266 Another result which neared statistical significance was no pain with strenuous or very
267 strenuous activity (p=0.08). To determine significance of this variable would have required
268 70 subjects in each group and thus we are underpowered to appropriately examine this
269 variable. Cohort size is certainly a limitation and we are unable to conclude a difference on
270 this variable. However, without any significant differences in examination including effusion,
271 range of movement or stability as well as that an equivalent number of patients returned to,

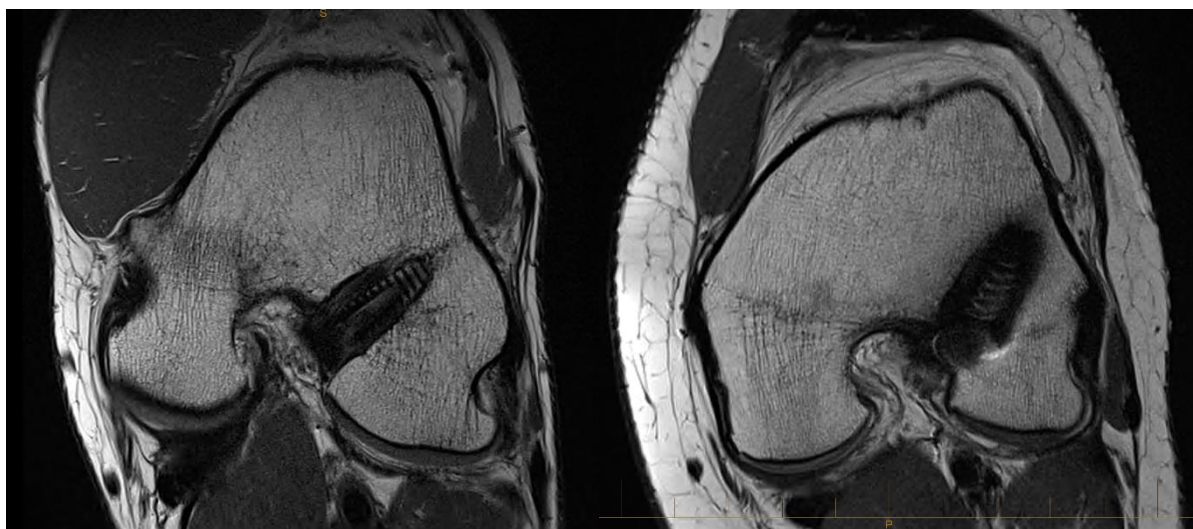
272 at a minimum, strenuous level activity, it is difficult to determine what the source of pain
273 may be for 17% of patients in the PEEK group.

274 One of the benefits of PEEK is that it does not interfere with post-operative imaging on MRI.
275 This is indicated in the superior inter-observer reliability in measuring tunnel volumes for
276 PEEK compared to titanium screws. Particularly on measuring the femoral tunnels with
277 titanium, the reliability was graded as moderate agreement as per Landis and Koch criteria
278 compared to substantial in the PEEK group. This is likely secondary to the degree of scatter
279 artifact caused by metal material. A further benefit is that compared to bioabsorbable
280 screws, PEEK does not cause cysts or inflammatory change due to degradation, showing
281 comparable results to titanium. Furthermore, in the case of revision surgery the PEEK screw
282 can be removed with the same ease of titanium as, unlike bioabsorbable screws, PEEK does
283 not lose structural integrity over time.

284 There was noted to be a high rate of effusion identified on MRI in the titanium and PEEK
285 groups at 76% and 67% ($p=0.3$). Effusions were graded to be small and the incidence of
286 associated synovitis was relatively low, 22% and 10% for Titanium and PEEK groups
287 respectively. It has previously been reported that at 12-months only 11% of patients will
288 have a knee joint effusion back to baseline ¹⁵. Therefore, this rate of MRI reported effusion
289 may be expected at 12-month review. It is noted that at clinical review at 24 months, 94%
290 and 86% of patients in the Titanium and PEEK group had no clinically apparent effusion.

291 There was found to be a significant difference between the titanium and PEEK screw groups
292 in regards to the proportion of patient who demonstrated incomplete graft integration on
293 the femoral side. This finding was seen in six of the 61 patients (10%) in the PEEK group, and

294 none of the 55 patients from the titanium group. Incomplete integration was defined as
295 focal or diffuse high signal in the graft adjacent to the interference screw, if this was not
296 observed then it was categorized as complete integration. It is likely that the difference in
297 femoral integration is attributable to the inability to assess graft signal in the presence of
298 metal artifact caused by the titanium screw, despite the use of suppression software. This
299 concept can be seen below by comparing representative MRI slices from a titanium and
300 PEEK screw patient (Figure 3). It can be seen that the graft is directly adjacent to the screw
301 and obscured by metal artifact in the titanium screw group.. There was, however, no
302 significant difference in the rates of complete integration for the tibia. Artifact produced by
303 metal in MRI scan is related to, amongst other things, the orientation of the implant in the
304 magnetic field²³. It is believed that the oblique orientation of the screw in the femoral
305 tunnel results in a greater degree of artifact and difficulty in visualizing the graft. It is our
306 impression that the result of incomplete integration of the graft at the femur in the PEEK
307 group is unlikely to accurately represent a true difference in behaviour of the grafts about
308 the two screw types, but rather an inferior ability to accurately view the graft adjacent to
309 the metal screws.



310

311 Figure 3: Comparison of MRI appearance of bone adjacent to a PEEK (3a) and titanium (3b)
312 screw, highlighting interference phenomenon caused by metallic properties of titanium
313 which reduces the ability to visualise the adjacent tunnel and ACL graft
314

315 It was also found that there was a significant difference in the tunnel volume of the femur
316 with the titanium tunnel being significantly wider ($p=0.002$). As with the difficulty of
317 interpreting complete femoral integration, it was particularly difficult to measure the true
318 volume of the femoral tunnel with the metal artifact. This can also be illustrated with the
319 rates of inter-observer reliability. There was less consistence in measuring of the femoral
320 tunnels compared to the tibial tunnels; 0.689 and 0.531 for PEEK and titanium on the femur,
321 compared to 0.868 and 0.768 on the tibia. Measurement of the femoral tunnel with the
322 titanium screw had only a moderate ICC, this is possibly due to the obliquity of the tunnel
323 within the femur and its tangential course to the cortical margin. The tibial tunnel runs
324 deeply with the tibal and thus is easier to define.

325

326 This study demonstrates a novel volume assessment technique for tibia and femoral tunnels
327 and show that the absence of signal flare on MRI from the PEEK screws greatly improved
328 inter-observer reliability. There are several techniques suggested in the literature for the
329 assessment of tunnel size^{1, 7, 10-12, 17, 24, 25} with CT scan typically seen as the gold standard^{8, 17}.
330 However, ICC for CT scan has previously been reported as only 0.49-0.76 for intra and inter-
331 observer reliability¹⁸. In most clinical settings, sufficient information regarding tunnel size
332 and widening can be gathered from plain radiographs to allow planning of revision surgery.
333 Where quantitative volume assessment is important, for example in the setting of research,
334 given the combination of higher accuracy, absence of radiation, and additional soft tissue
335 information garnered, we feel tunnel volume assessment is best done with MRI. Mayr et. al

336 also measured tunnel volume on 1.5T MRI however with measurements off of the axial
337 slice, rather than our technique of slices perpendicular to the tunnel ¹⁷. For the tibia they
338 found almost identical ICC of 0.869. Similar to our findings, the ICC for the femur was lower
339 than that of the tibia. Although they reported a higher rate of ICC, we feel that due to the
340 trajectory of the femoral tunnel, a perpendicular oblique view on a 3T scanner shows a
341 greater number of slices with the tunnel visible and better reflects the true tunnel volume.
342 The technique presented here can be used with standard MRI scanners and requires only
343 modification of the orientation of the acquired slices.

344 From this study we conclude equivalent clinical outcomes of PEEK interference screws
345 compared to titanium. The use of PEEK interference screws in ACL reconstruction provides a
346 stable, reliable method of fixation. There is no significant difference in subjective measures,
347 objective examination or graft reinjury at two year follow up when compared with titanium
348 interference screws. MRI assessment at one year showed equivalent rates of effusion,
349 synovitis, ligamentization and cyst formation, and the absence of signal flare on PEEK MRI
350 images allowed for reproducible tunnel volume measurements and adequate assessment of
351 the graft in the tunnels. The PEEK screw is an alternative to the gold standard of titanium
352 screw in ACL reconstruction, may simplify revision procedures and allow for superior
353 imaging of the tunnel and graft. PEEK interference screws are now our preferred method of
354 fixation for ACL reconstruction.

355

356

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